Scaling laws between the hydrodynamic parameters and molecular weight of linear poly(2-ethyl-2-oxazoline)\textsuperscript{†}

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Poly(2-ethyl-2-oxazoline) (PEtOx), as an alternative polymer to poly(ethylene glycol), has potential applications in biomedical fields. The hydrodynamic parameters, such as the hydrodynamic radius and sedimentation coefficient, are important to understand its dynamics and properties, including its effect on the interactions between proteins and cells. In this study, we have investigated the hydrodynamic properties and thermodynamic parameters of a series of narrowly distributed PEtOx polymers with molecular weights ranging from $1.3 \times 10^6$ to $3.1 \times 10^6$ g mol\textsuperscript{−1}, and the scaling laws between them by the use of a combination of analytical ultracentrifugation and laser light scattering. It is found that the sedimentation coefficient ($s_{20,w}$) and hydrodynamic radius ($R_{h,0}$) at infinite dilution scale with molecular weight ($M_w$) as $s_{20,w} = K_s \times M_w^{0.0771 (S) \times M_w^{0.462 \pm 0.019}}$ and $R_{h,0} = K_R \times M_w^{0.0179 (nm) \times M_w^{0.539 \pm 0.012}}$, respectively.

Introduction

Polyethylene glycol (PEG) has received great interest in the pharmaceutical industry because PEG is nontoxic, biocompatible and is approved by the FDA.\textsuperscript{1−4} It is well known that the covalent attachment of PEG to proteins (i.e. PEGylation) can increase the circulating half-life in blood by increasing the stability of the proteins, as well as by reducing the renal ultrafiltration.\textsuperscript{2−4} Normally, PEGylation can reduce the immunogenicity of some proteins.\textsuperscript{5} However, due to the wide use of PEG in biomedical applications, recently more and more anti-PEG antibodies have been reported.\textsuperscript{6−8} Thus, drug companies are eager to find alternative polymers. Among the alternative polymers, poly(2-ethyl-2-oxazoline) (PEtOx) is a promising candidate because of its low toxicity and immunogenicity.\textsuperscript{9−17}

The chemical structures of PEtOx and PEG are shown in Fig. 1.

In order to reduce kidney filtration, the hydrodynamic radius ($R_h$) of the PEtOx–protein conjugate should be larger than the size of the glomerular basement membrane, which is in the range of 2.5−5 nm.\textsuperscript{18} Based on the extensive data from the pharmacokinetic studies of PEG–protein conjugates, a possible way is to replace PEG by PEtOx, which has the same hydrodynamic radius. Recently Armstrong et al. found that the hydrodynamic radii of nonionic polymers and proteins are the principal determinant of their effect on red blood cell aggregation.\textsuperscript{19} Moreover, Sim et al. have reported that the precipitation efficiency of PEG is mainly determined by the hydrodynamic radius.\textsuperscript{20} These studies further indicate that knowing the relationship between $R_h$ and the molecular weight of PEtOx can help us to explain the effect of PEtOx on the interactions between cells and proteins. The solution properties of a series of PEtOx polymers with molecular weights ranging from $6.8 \times 10^4$ g mol\textsuperscript{−1} to $9.14 \times 10^5$ g mol\textsuperscript{−1} in THF have been studied by light scattering and viscometry.\textsuperscript{21} While most biomedical applications of PEtOx are in aqueous systems, the aqueous solution properties of PEtOx with a wide range of molecular weights, taking into account the hydrodynamic radius, need to be examined systematically.

In this article, a series of PEtOx polymers with molecular weights from $1.3 \times 10^5$ to $3.1 \times 10^5$ g mol\textsuperscript{−1} was obtained by the fractionation of a linear commercial PEtOx sample by gel
permeation chromatography (GPC) or by the cationic ring-opening polymerization of the monomer 2-ethyl-oxazoline. Both analytical ultracentrifugation (AUC) and laser light scattering (LLS) were used to characterize the PEtOx samples. For two linear PEtOx samples with lower molecular weights, both AUC and LLS give similar results regarding the $R_h$ and weight-average molecular weight ($M_w$). However, because of the low scattering intensity, the concentration of PEtOx used in the LLS experiments was much higher than that used in AUC to obtain reliable results. Possibly for the same reason, Sung and Lee did not report the hydrodynamic radius of PEtOx samples with molecular weights of less than $1.41 \times 10^5$ g mol$^{-1}$ in THF.\textsuperscript{24} Our objective is to understand the scaling of the molecular weight-dependent hydrodynamic parameters of PEtOx in aqueous solution.

Experimental

Materials

Linear poly(2-ethyl-2-oxazoline), with a weight-average molar mass of 500 000 g mol$^{-1}$, was purchased from the Sigma-Aldrich Company, Inc. and used as received as a starting material for fractionation. The commercial linear PEtOx sample was carefully fractionated by GPC. Briefly, 50 μL of PEtOx tetrahydrofuran (THF) solution with a concentration of 20 mg mL$^{-1}$ was injected into steam from a sample loop. According to the principle of GPC, it takes a shorter time for the high-molecular-weight polymers to reach the column outlet. Fractions were collected at 1 mL intervals from the chromatography. The same procedure was repeated ten times to obtain sufficient samples. Then, the THF solvent was evaporated under reduced pressure. The aqueous solution of each PEtOx fraction was prepared by dissolving the PEtOx fraction in 0.6 mL Milli-Q water. Two PEtOx samples with lower molecular weights were synthesized by the cationic ring-opening polymerization of the monomer 2-ethyl-2-oxazoline. In brief, 2-ethyl-2-oxazoline (99%, Sigma-Aldrich) was dried over calcium hydride and distilled under reduced pressure prior to use. Methyl tosylate (98%, Sigma-Aldrich) was distilled under reduced pressure. Acetonitrile, the reaction solvent, was refluxed with and distilled from alkaline KMnO$_4$ and KHSO$_4$, followed by fractional distillation from calcium hydride. Methyl tosylate, EtOx and acetonitrile were added into a glass tube. After three freeze-vacuum-thaw cycles, the tube was sealed under vacuum and then placed in a thermostat at 80 °C for 24 h. The PEtOx-acetonitrile solution was added to sodium carbonate aqueous solution. The mixture was stirred for 16 h at 90 °C and extracted three times with chloroform after cooling to room temperature. The organic phases were dried over sodium sulfate and filtered. Then, the solvent was evaporated under reduced pressure and the resultant PEtOx was dried under reduced pressure. The $^1$H-NMR spectra of these two PEtOx samples were recorded in CDCl$_3$ using a Bruker 300 MHz spectrometer.

Laser light scattering

A commercial laser light scattering spectrometer (ALV/DLS/SLS-5022F) equipped with a multi-τ digital time correlator (ALV5000) and a cylindrical 22 mW UNIPHASE He–Ne laser ($λ_0 = 632.8$ nm) was used. In static LLS,\textsuperscript{22,23} the weight-average molar mass ($M_w$) and the z-average root-mean square radius of gyration ($〈R_g^2〉^{1/2}$) in a solution from the angular dependence of the excess absolute scattering intensity which is known as the excess Rayleigh ratio [$R_{ex}(q)$] can be obtained by using

$$\frac{KC}{R_{ex}(q)} \approx \frac{1}{M_w} \left(1 + \frac{1}{3} \left(\frac{R_g}{q}\right)^2\right) + 2A_2C$$

where $K = 4π^2n^2(dn/dc)^2/(N_Aλ_0^4)$ and $q = (4πn/λ_0)\sin(θ/2)$ with $C$, $dn/dc$, $N_A$, and $λ_0$ representing the concentration of the polymer, the specific refractive index increment, Avogadro’s number and the wavelength of light, respectively. $A_2$ is the second virial coefficient. The refractive index increment ($dn/ dc = (0.161 \pm 0.001)$ mL g$^{-1}$) of PEtOx in water was measured with a precise differential refractometer at 20 °C and 633 nm.\textsuperscript{24} In dynamic LLS,\textsuperscript{25} the Laplace inversion of a measured intensity-intensity time correlation function $G^{(2)}(t,q)$ in the self-beating mode can result in a line-width distribution $G(Γ)$. For a pure diffusive relaxation, $Γ$ is related to the translational diffusion coefficient $D$ by $Γ/q^2 = D$ at $q \rightarrow 0$ and $C \rightarrow 0$, or a hydrodynamic radius $R_h = k_BT/(6πηD)$ with $k_B$, $T$, and $η$ representing the Boltzmann constant, the absolute temperature and the solvent viscosity, respectively. Each PEtOx aqueous solution was repeatedly filtrated using a peristaltic pump (Masterflex®; Model 77390-00, Cole–Parmer Instrument Co.) and a 0.45-μm hydrophilic PTFE filter.

Sedimentation velocity analysis

Sedimentation velocity assays were performed using a Proteomelab XL-A/XL-I analytical ultracentrifuge (Beckman Coulter Instruments) with an An-60 Ti rotor, one cell assembled with sapphire windows, a double-sector 12 mm length charcoal-filled Epon centerpiece and an interference optics detector. All of the experiments were conducted at 60 000 rpm and 20 °C. 400 μL of the PEtOx fraction solution was loaded for measurement with 410 μL of water as the reference. Data were collected using the software provided with the instrument, and analyzed using the SEDFIT (version 12p44) program.\textsuperscript{26,27} The partial specific volume ($v$) of PEtOx in aqueous solution was measured by a DMA4500 densitometer (Anto Paar) at 20 °C. The value of $v$ was 0.85 mL g$^{-1}$, which is close to the value ($v = 0.87$ mL g$^{-1}$) reported by Chen et al.\textsuperscript{28} As the partial specific volume usually does not have molecular weight dependence, we used this value for all of the PEtOx fractions.\textsuperscript{26}

Results and discussion

It is known that narrowly distributed linear poly(2-ethyl-2-oxazoline) with molecular weights ranging from 1 to ~50 kg mol$^{-1}$ can be synthesized by conventional thermal heating and microwave-assisted cationic ring-opening polymerization.
However, it is still difficult to obtain narrowly distributed linear PETOx with a molecular weight greater than 50 kg mol⁻¹. Our preliminary results showed that the distribution of the PETOx samples fractionated by the dissolution–precipitation process in a mixture of dry THF and dry n-hexane were not narrow enough for AUC experiments.34 Thus, in this study we used GPC to fractionate a commercial linear PETOx sample. Owing to the advantage of AUC experiments that only small amounts of PETOx samples (~0.2 mg) are needed, here only analytical GPC was used. Two PETOx samples with molecular weights of 1.3 kg mol⁻¹ and 3.3 kg mol⁻¹ were synthesized by conventional thermal heating CROP.

Fig. 2 shows the sedimentation coefficient distributions of five PETOx fractions in aqueous solution, analyzed with the continuous c(s) distribution model by SEDFIT software. From Fig. 2, we know that the distributions of all of the fractions are narrow. Note that for the PETOx-3 and PETOx-4 fractions, small amounts of polymers with higher sedimentation coefficients exist in each fraction. This means that the polymers with a higher s, which may have the same hydrodynamic radius as the majority of the fractions, can not be fractionated by GPC.

Besides using the c(s) model, the c(s, ff0) model has also been used to analyze the data.27 Note that from the c(s, ff0) model, the polydispersity index (M_w/M_n) can be obtained. The corresponding results are summarized in Table 1. From Table 1, we know that the difference between the M_w values from these two models is less than 10% and the distributions of all of the fractions are narrow.

Due to solute–solute interactions and the shapes of the macromolecules differing from spherical, the hydrodynamic parameters (such as the sedimentation coefficient and hydrodynamic radius) may have a concentration dependence. In order to eliminate this effect, the concentration dependence of sedimentation coefficient and hydrodynamic radius was investigated. Because of the limited amount of the PETOx fractions, less than 1 mg, the concentration of the PETOx solutions can not be determined by a conventional balance. As we used interference optics as the detector and a triggerable laser diode as the light source, the relationship between the shift of the interference fringes (J) and the concentration of the solution (C) can be described as

\[ J = \frac{a(dn/dc)}{\lambda} C \]

Table 1 Characterization of the PETOx samples used

<table>
<thead>
<tr>
<th>Sample</th>
<th>M_w (g mol⁻¹)</th>
<th>c(s)</th>
<th>c(s, ff0)</th>
<th>M_w/M_n</th>
</tr>
</thead>
<tbody>
<tr>
<td>PETOx-1</td>
<td>1300</td>
<td>1190</td>
<td>1.01</td>
<td></td>
</tr>
<tr>
<td>PETOx-2</td>
<td>3230</td>
<td>3470</td>
<td>1.10</td>
<td></td>
</tr>
<tr>
<td>PETOx-3</td>
<td>6890</td>
<td>7470</td>
<td>1.04</td>
<td></td>
</tr>
<tr>
<td>PETOx-4</td>
<td>14 300</td>
<td>15 300</td>
<td>1.14</td>
<td></td>
</tr>
<tr>
<td>PETOx-5</td>
<td>25 300</td>
<td>26 850</td>
<td>1.17</td>
<td></td>
</tr>
<tr>
<td>PETOx-6</td>
<td>53 600</td>
<td>57 620</td>
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</tr>
<tr>
<td>PETOx-8</td>
<td>313 100</td>
<td>277 000</td>
<td>1.58</td>
<td></td>
</tr>
</tbody>
</table>

* Analyzed by the c(s, ff0) model. The relative error of the M_w is ±3%.

We know that when the molecular weight is below ~5 × 10⁴ g mol⁻¹, both s and R_h do not change with concentration, and the extrapolation of s and R_h to zero concentration leads to s_0 and R_h,0 at infinite dilution. Note that Luo et al. reported that for PEG, when the molecular weight is less than 6 × 10⁴ g mol⁻¹, s shows no dependence

Fig. 2 Sedimentation coefficient (s) distributions of PETOx-1, PETOx-2, PETOx-3, PETOx-4, and PETOx-8 at 20 °C. Where the corresponding concentrations of the samples are 0.6 mg mL⁻¹, 0.6 mg mL⁻¹, 0.2 mg mL⁻¹, 0.3 mg mL⁻¹ and 0.5 mg mL⁻¹, respectively.

Fig. 3 Concentration dependence of the sedimentation coefficients of PETOx-5, PETOx-6, PETOx-7, and PETOx-8 at 20 °C.
on molecular weight. The difference between these two polymers implies that for the same molecular weight, the interactions between PEG molecules are larger than that between PEtOx molecules, which is possibly due to the larger hydrodynamic volume of PEG.

Besides sedimentation velocity (SV) experiments, we also used a combination of static and dynamic light scattering to characterize the PEtOx aqueous solutions. Fig. 5 shows that the intensity–intensity time correlation functions of the PEtOx-2 aqueous solution contains two relaxation modes. The faster mode corresponds to the pure diffusion of single PEtOx-2 chains and the slower relaxation mode may be related to the loosely-assembled aggregates due to the remaining hydrophobic tosyl end group. Our results show that the slow mode can be removed by repeated filtration for 2 h. Note that it is important to remove the slow mode for the measurement of the molecular weight and the hydrodynamic radius of PEtOx, especially for the PEtOx samples with smaller \( M_w \). In our study, the same process was used for the characterization of two synthesized samples, PEtOx-1 and PEtOx-2.

Fig. 6 and Fig. 7 show typical Zimm plots and the hydrodynamic radius distribution of PEtOx-1, respectively. The extrapolation of \( KC/R_{vv}(q) \) to \( C \to 0 \) and \( q \to 0 \) leads to a value of \( M_w = 1.27 \times 10^3 \) g mol\(^{-1}\) which is close to the value of \( M_w = 1.30 \times 10^3 \) g mol\(^{-1}\) determined by the SV experiments. The slope for the line plotting \( KC/R_{vv}(q)q^2 \) versus \( C \) gives the value of \( A_2 = (2.2 \pm 0.7) \times 10^{-3} \) mol mL g\(^{-2}\), indicating that water is a good solvent for PEtOx. Due to the small size of PEtOx-1 in comparison with the wavelength of the laser light, there is no angular dependence of \( KC/R_{vv}(q) \). Thus it is difficult to obtain a reliable \( <R_h> \) of PEtOx-1. The distribution of the hydrodynamic radius shows that PEtOx-1 is narrowly distributed and \( <R_h> = 0.95 \) nm, which is also consistent with the value determined by the SV experiments (\( <R_h> = 0.95 \) nm).

Note that the scattering light intensity is proportional to the square of the mass of a single scattering object. In order to obtain a large enough scattering light intensity, \( \sim 500 \) mg of PEtOx-1 was needed to determine the accurate molecular weight and \( R_h \) as the molecular weight of PEtOx-1 is as small as \( \sim 1.3 \times 10^3 \) g mol\(^{-1}\).

Fig. 8 shows that there is a scaling relationship between \( s_{20,w} \) and \( M_w \) when \( M_w \) is in the range of \( 1 \times 10^3 \) g mol\(^{-1}\) and 4
The scaling index is \( \alpha = 0.462 \pm 0.019 \), which is between 0.4 and 0.5, indicating that PEtOx polymers adopt a random coil conformation in aqueous solution.\(^{39}\) Luo et al. reported that for PEG, the sedimentation coefficient \( S_0 \) scales to \( M_w \) as \( S_{20,w} = K_s \times M_w^{\alpha} = 0.0068 \) (S) \( \times M_w^{0.462 \pm 0.019} \). The scaling index \( \alpha \) for PEtOx is similar to that of PEG, implying that both of the polymers adopt the same conformation in water. Fig. 8 also shows a transition of the scaling laws. The results show that values of \( \alpha_1 = 0.559 \pm 0.016 \) and \( \alpha_2 = 0.394 \pm 0.010 \) were obtained for \( M_w < 2 \times 10^4 \text{ g mol}^{-1} \) and \( 2 \times 10^4 \text{ g mol}^{-1} < M_w < 4 \times 10^4 \text{ g mol}^{-1} \), respectively. It should be noted that the scaling index is typically around 0.67 for a compact sphere, 0.4–0.5 for a random coil and 0.15 for a rigid rod.\(^{40}\) The parameters from the five samples with higher \( M_w \) are lower than the four samples with lower \( M_w \), indicating that the PEtOx samples with higher \( M_w \) adopt a more extended coil conformation.

Both Chen et al. and Ambreen et al. studied the phase transition of the PEtOx aqueous solution by laser light scattering.\(^{34,41}\) Chen et al. reported that the \( \langle R_h \rangle \) of PEtOx polymer with a molecular weight of 1.16 \( \times 10^5 \text{ g mol}^{-1} \) was 10.7 nm at 30 °C which was lower than their cloud point.\(^{41}\) Ambreen et al. characterized a narrowly distributed PEtOx fraction by a combination of static and dynamic light scattering and showed that the \( \langle R_h \rangle \) of this fraction with a \( M_w \) of 8.7 \( \times 10^5 \text{ g mol}^{-1} \) was 29 nm.\(^{34}\) We have combined their data together with our data in this study in Fig. 9 to show the molecular weight dependence of \( R_h \). From Fig. 9, we know that \( R_{h,0} = K_{R_h} \times M_w^{\beta} = 0.0179 \) (nm) \( \times M_w^{0.539 \pm 0.012} \). Note that for real polymer chains in a good solvent and a theta solvent, the scaling indexes are 0.59 and 0.5, respectively.\(^{42}\) Recently, using a coarse-grained molecular dynamics simulation, Wang et al. reported that the radius of gyration of poly(ethylene terephthalate) scales with the degree of polymerization with a scaling index of 0.50, which is very close to the theoretical value. The scaling index obtained in our study is between the values predicted for in the good solvent and the theta solvent.\(^{43-45}\)

Moreover, the sum of \( \alpha \) and \( \beta \) is 1.001, which is reasonable because from the Svedberg equation we know that \( M^2 \propto s/D \propto s/R_h \propto (K_s/M_w) \propto (K_{R_h} M_w^{-\beta}) \propto (K_S K_{R_h}) \times M^{\beta + 1} \). Fig. 9 also shows the weight-average molecular weight dependence of the hydrodynamic radius of PEG in water and PEtOx in THF. For the same molecular weight of PEtOx and PEG, the hydrodynamic radius of PEG is higher than that of PEtOx. Based on their structures, as shown in Fig. 1, the reason that PEG has a higher hydrodynamic radius may be due to its more favorable interaction with water molecules, and a larger degree of polymerization because the repeating unit of PEG has a smaller molar mass. Moreover, it is obvious that water is a better solvent for PEtOx than THF because for the same \( M_w \), the \( R_h \) in water is much larger than that in THF. Knowing the scaling law between \( R_h \) and molecular weight can help us to choose PEtOx polymers with an appropriate molecular weight. For example, Armstrong stated that nonionic polymers with a \( R_h \) less than 4 nm can inhibit red blood cell aggregation and those with a \( R_h \) larger than 4 nm can enhance the aggregation.\(^{19}\)

Based on Fig. 9, we know that the \( R_h \) of a PEtOx polymer with a molecular weight of 2.3 \( \times 10^4 \text{ g mol}^{-1} \) is 4 nm. Furthermore, if we consider that the interactions between PEtOx and proteins is similar to those between PEG and proteins, we can replace PEG with PEtOx of the same hydrodynamic radius, according to the scaling laws between the \( R_h \) and \( M_w \) of the two polymers. For instance, for three approved PEG conjugates (PEG-growth hormone receptor antagonist, PEG-interferon α2b and Pegfilgrastim), PEG polymers with molecular weights of 5 \( \times 10^4 \text{ g mol}^{-1} \), 1.2 \( \times 10^4 \text{ g mol}^{-1} \) and 2 \( \times 10^4 \text{ g mol}^{-1} \) have been used.\(^{5}\) We could choose PEtOx polymers which have the same \( R_h \) to replace the PEG polymers, that is, the corresponding molecular weights of PEtOx are 6.5 \( \times 10^4 \text{ g mol}^{-1} \), 1.7 \( \times 10^4 \text{ g mol}^{-1} \) and 2.8 \( \times 10^4 \text{ g mol}^{-1} \), respectively.
Conclusion

By the use of a combination of analytical ultracentrifugation and laser light scattering, the relationships between the hydrodynamic radius ($R_{h,0}$), the sedimentation coefficient ($s_{20,w}$) at infinite dilution and the molecular weight of a series of linear poly(2-ethyl-2-oxazoline) polymers in aqueous solution have been studied. Our results show that $R_{h,0}$ and $s_{20,w}$ scale with molecular weight ($M_w$) as $R_{h,0} = K_{R_{h,0}} \times M_w^{0.0179}$ (nm) $\times M_w^{0.539 \pm 0.012}$ and $s_{20,w} = K_s \times M_w^{0.0071}$ (S) $\times M_w^{0.462 \pm 0.0019}$, respectively, indicating that PETOx polymers adopt a random coil conformation in aqueous solution. Our findings will provide a guide for choosing PETOx polymers with an appropriate molecular weight for its pharmaceutical applications.

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